

Silicon Photomultipliers:

Introducing the **Silicon** age in
low light detection

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Part 2: applications (a limited number of)

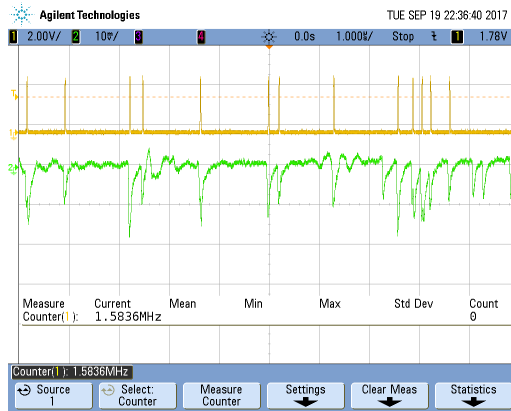
Rudjer Boskovic Institute
October 24th, 2018



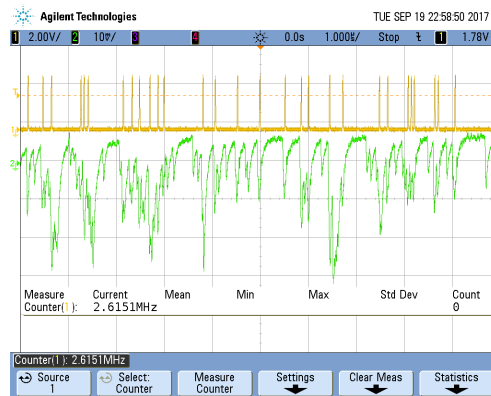
Benedetta Cappa Marinetti - Velocità di motoscafo, 1919

Applications (a limited number of)

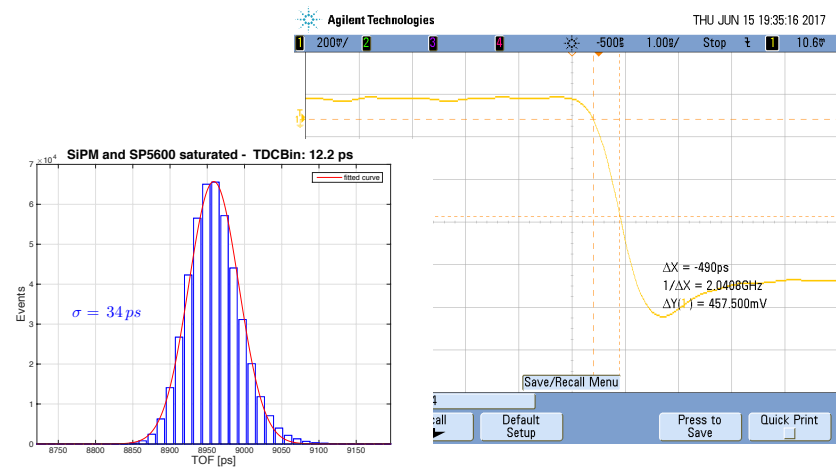
❖ Pulse mode:



❖ Current mode:

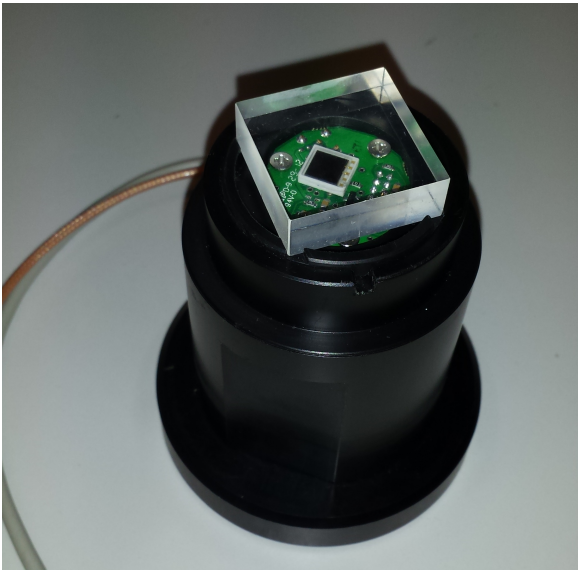


❖ Timing

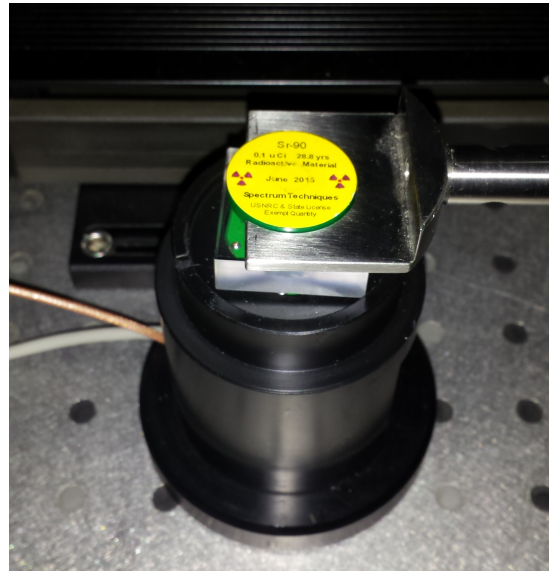


p.s. extremely biased by my activity & experience!

A Friday afternoon exercise (1/3):
Thickness measurement by β absorption (aka β gauging)



- ❖ 6x6 mm² SiPM
- ❖ 1 cm thick plastic scintillator



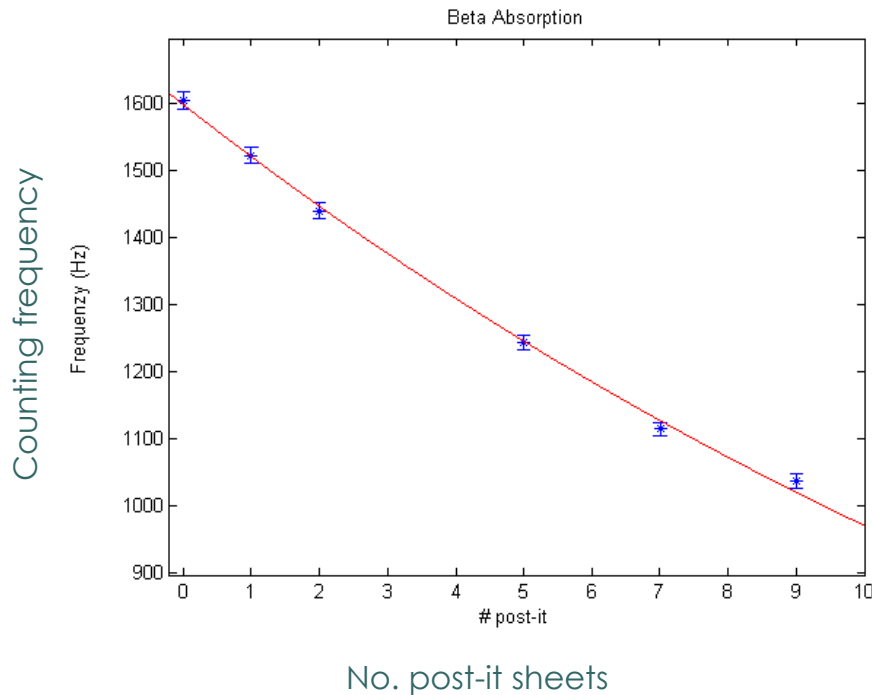
- ❖ 37 kBq ⁹⁰Sr source



- ❖ post-it sheets interleaved between the source and the scintillator

Can I count the number of sheets by the counting rate?

A Friday afternoon exercise (2/3):
Thickness measurement by β absorption (aka β gauging)



$$v = ae^{-bn}$$

$$a = 1600 \text{ Hz}$$

$$b = 0.05$$

n = number of post-it sheets

- in 250 ms I can tell you at 3σ level if I have 1 or 2 post-it
- In 25" I can detect a thickness variation at the 10% level

Is it serious?

A Friday afternoon exercise (2/3):

Thickness measurement by β absorption (aka β gauging)

Radioisotope sensor for measuring the density of paper and cardboard web based on the isotope Kr 85 A361 CAN LEB1



Brief description

Radioisotopic density sensor of sheet materials A361 CAN (LEB-1) is designed for use in automated quality control system "A-3000" for the continuous and non-contact technological control paper web density or other sheet materials.

Application range — paper web density continuous monitoring for the papermaking and other sheet materials process control.



5014i Beta Continuous Ambient Particulate Monitor

Measure PM-10, PM-2.5 or PM-1 mass concentrations with the Thermo Scientific™ 5014i Beta Continuous Ambient Particulate Monitor. The 5014i distinguishes itself from other beta measurement methods by utilizing a continuous (non-step wise) mass measurement with a proven industry standard which provides for long-term unattended operation. To accurately address potential water bias and volatile loss, the Dynamic Heating System allows the user to hold the sample temperature at a fixed value or below a relative humidity threshold.

Contact Sales

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Contact Support

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Radiation Protection – an exemplary illustration for the UK



The TN15™ high sensitivity thermal neutron detector utilizes a state-of-the-art Silicon photomultiplier (SiPM) and offers world-leading specification in a compact form. The TN15™ surpasses the performance of a 100mm long 13mm ³He tube at 4 atmospheres.

Specifications:

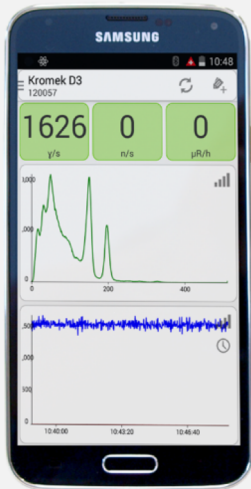
Equivalent to 100mm x 13mm Ø ³He at 4 atmospheres

Photo-sensor	SiPM array
Thermal Neutron Sensitivity	>50%
Maximum throughput	10,000 cps
Power consumption	250 mW
Dimensions	131mm x 33mm x 24mm
Weight	110 gram
Temperature range	-10 to 40°C

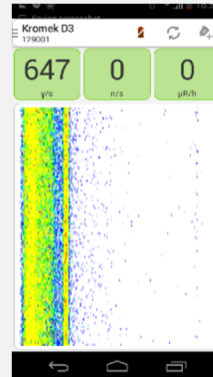
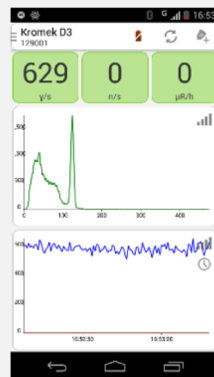
TN15™ by KROMEK, Sedgefield
County Durham, UK
www.kromek.com

The 2015 blockbuster

D3S



- Compact Bluetooth gamma neutron detector for \$400
- All technology available at OEM level
 - Gamma module
 - Neutron module
 - Bluetooth MCA
 - All designed for ultra low power
- All software can be supplied badged or further developed as required
 - Android application
 - Fully secure web application including GPS

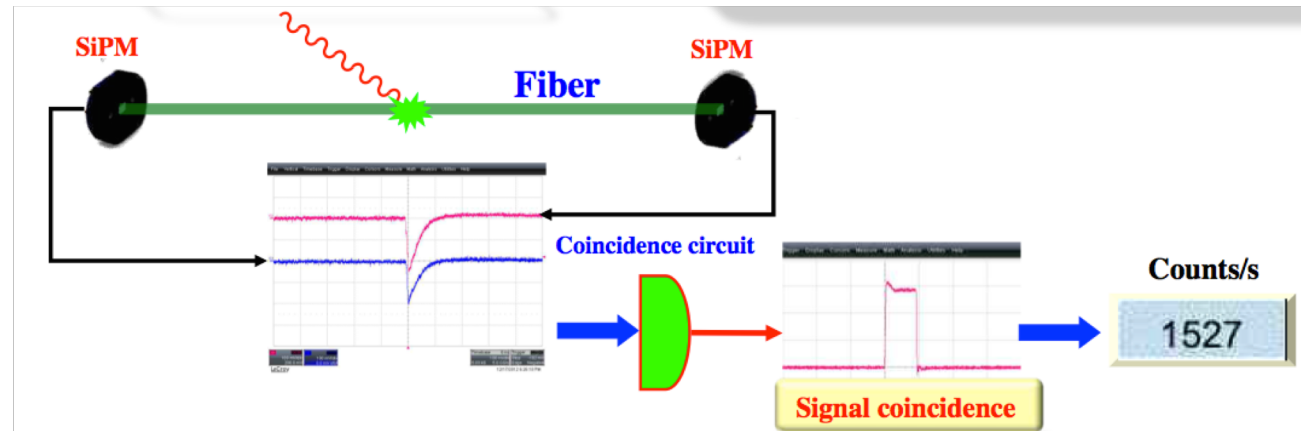


About Nuclear Waste

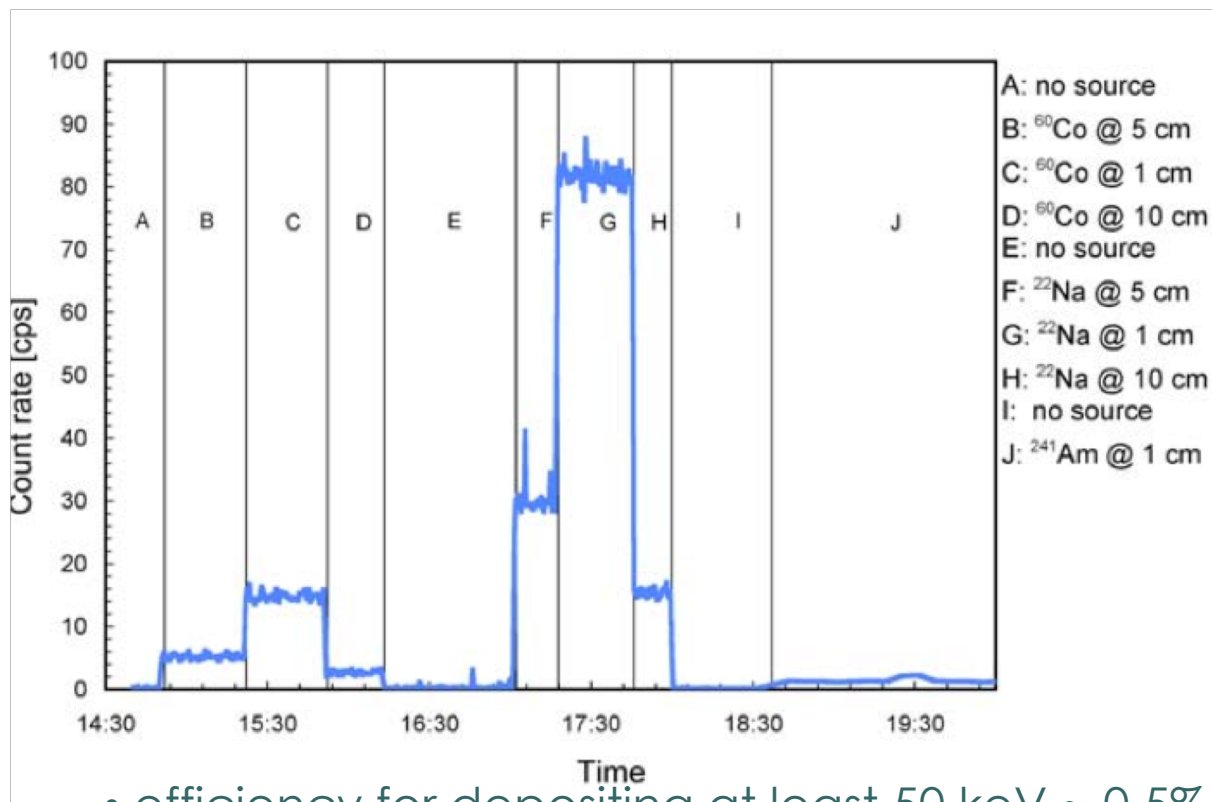
Paolo Finocchiaro, Nuclear Physics News,
<http://dx.doi.org/10.1080/10619127.2014.941681>



- ❖ **Goal:** online monitoring of radiation emitted by nuclear waste drums
- ❖ **Method:** “annular” detector, made out of a plastic scintillating fiber connected to SiPM at both ends



Qualification results:

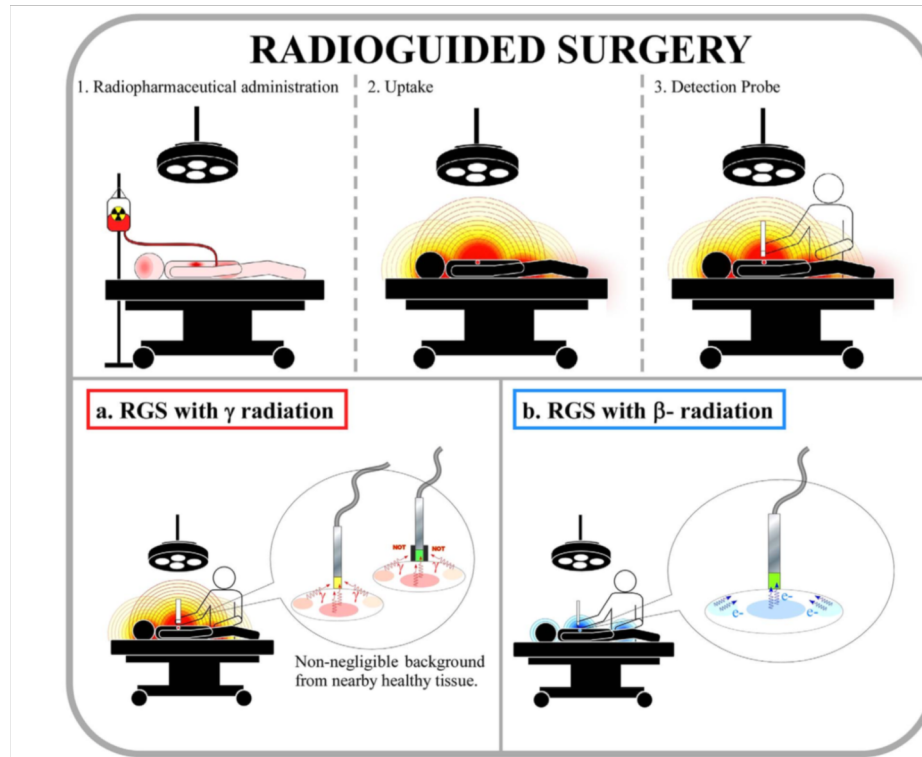


- ❖ ^{60}Co , 35 kBq
- ❖ ^{22}Na , 243 kBq
- ❖ ^{241}Am , 36 MBq
- ❖ ^{137}Cs , 231 kBq

- efficiency for depositing at least 50 keV $\sim 0.5\%$
- mean deposited energy ~ 180 keV, i.e. 1800 photons (light yield $\sim 10^4$ photons/MeV)
- mean detected signal ~ 40 photo-electrons
- random coincidence rate ~ 1 Hz

RadioGuided Surgery (RGS)

1. F Bogalhas et al., Phys. Med. Biol. 54 (2009) 4439–4453
2. Solfaroli Camillocci et al., NATURE SCIENTIFIC REPORTS | 4 : 4401 | DOI: 10.1038/srep04401 (2014)
3. H. Sabet et al., IEEE TRANSACTIONS ON NUCLEAR SCIENCE, VOL. 62, NO. 5, OCTOBER 2015



The precise localization and complete surgical excision of tumors are one of the most important procedures in the treatment of cancer. In that context, the goal is to develop new intra-operative probes to help surgeons to detect malignant tissues previously labeled with β or γ radiotracers.

RGS with β^- (ref.2)

Focused on brain tumor (meningioma) for two reasons:

- It is particularly receptive to synthetic somatostatin analogues, such as DOTATOC, that can be labelled with the β^- emitting ^{90}Y
- The concentration of “standard” β^+ emitting isotopes (e.g. ^{18}F -FDG used for PET) is quite high in the brain, inducing a significant background

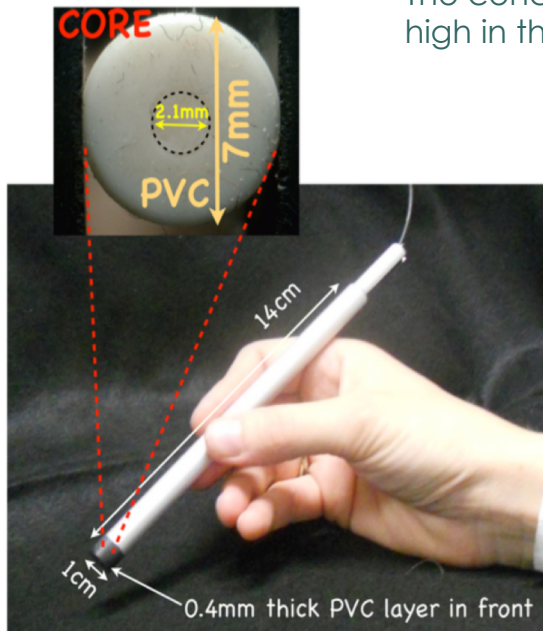


Figure 2 | First prototype of the intraoperative β^- probe. The core is a cylindrical scintillator (diameter 2.1 mm, height 1.7 mm) of polycrystalline p-terphenyl. A ring of PVC wraps the scintillator and shields it against radiation coming from the sides. The device is encapsulated inside an easy-to-handle aluminum body as protection against mechanical stress and it is protected against light by a thin PVC layer.

Results from phantoms with a specific activity corresponding to what can be expected in clinical applications

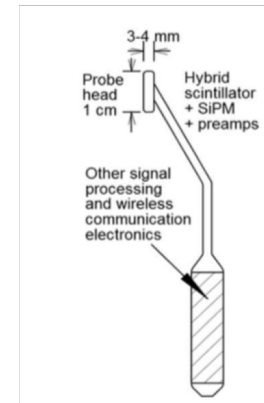
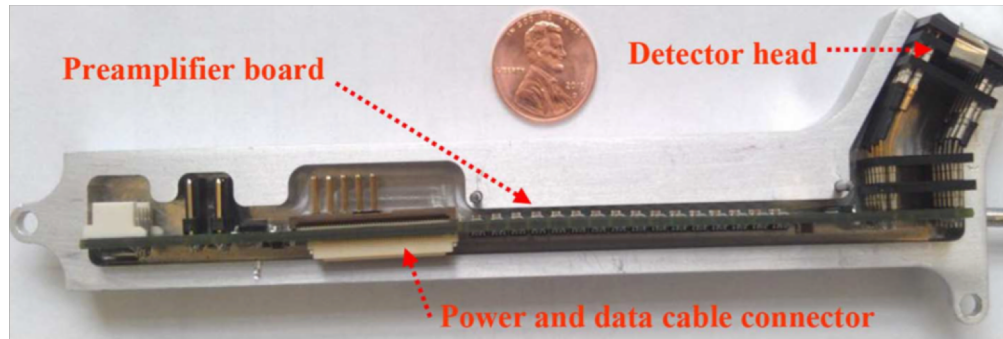
Phantom	Diameter (mm)	Height (mm)	Volume (ml)	Rate (cps) 22 kBq/ml	T (s) 22 kBq/ml	Rate (cps) 5 kBq/ml	T (s) 5 kBq/ml
Residual	6	3.5	0.10	31.6	1	6.6	2
H1	4	1	0.01	12.4	2	2.6	>10
H2	4	2	0.02	17.7	1	3.7	4
H3	4	3	0.04	20.1	1	4.2	4

Time required to get False Negative < 5% and False Positive \approx 1%

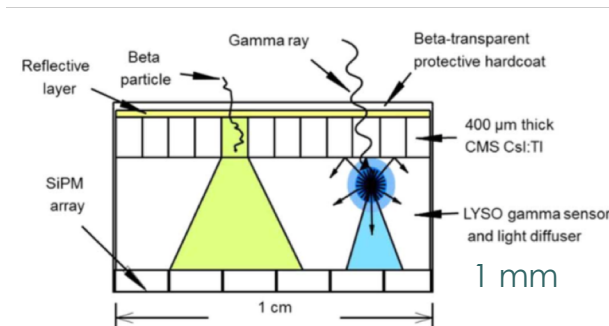
RGS with β^+ (ref.3) (1/2)

An IMAGING DEVICE engineered to detect β^+ emitting isotopes irrespective from the γ background

❖ Conceptual design & prototype of the probe



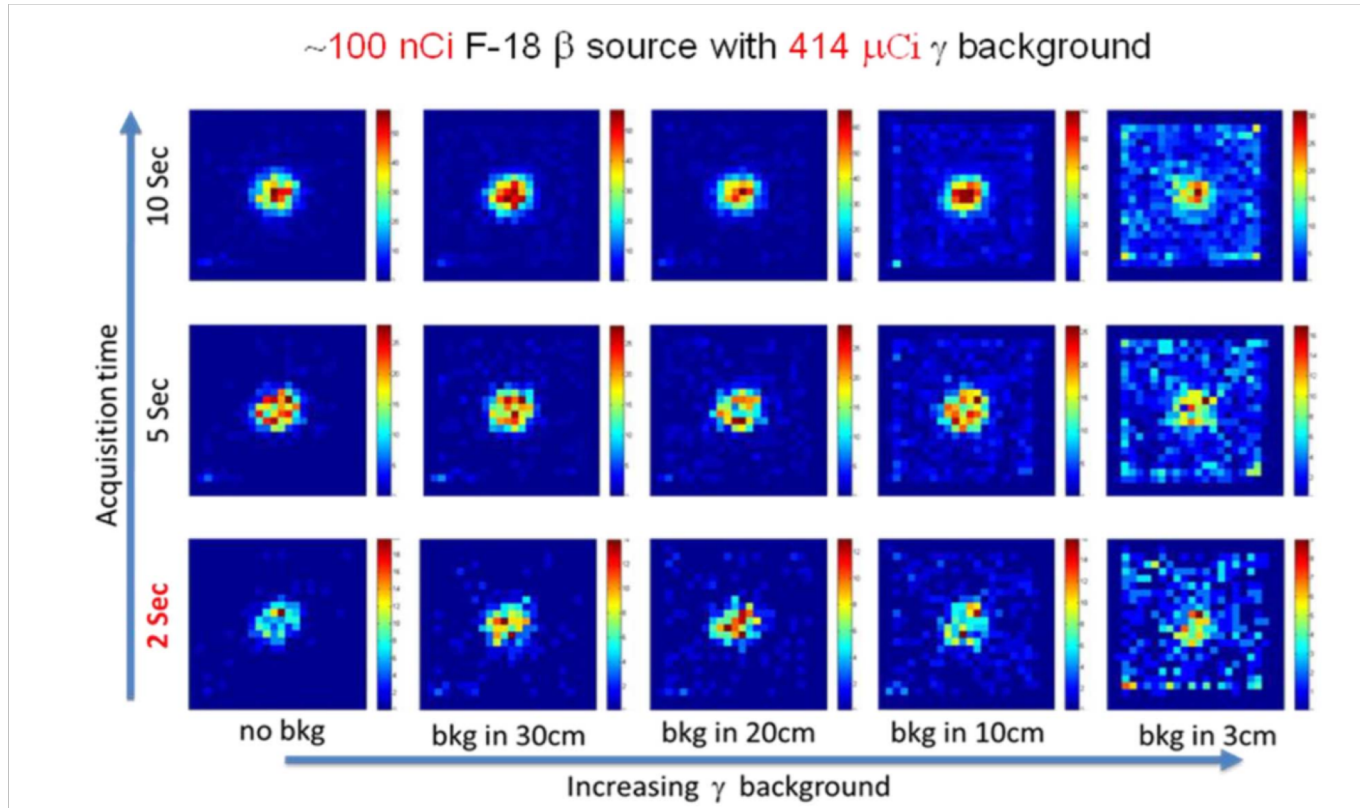
❖ A head designed to identify and discriminate β^+ from γ



- CsI to detect β^+ rather than plastic scintillator for the light yield (53 photons/keV vs 10 photons/keV); $\bar{E}_{\beta^+} = 250 \text{ keV}$, $E_{max} = 635 \text{ keV}$
- β^+ vs γ discrimination profiting from the difference in the time constant of the CsI (800 ns) vs LYSO (40 ns)

RGS with β^+ (ref.3) (2/2)

Images of a ^{18}F droplet ($\approx 1\text{mm diameter}$) @different background levels



Still a bit qualitative (on spatial resolution and sensitivity) but definitely intriguing



Response to a constant flux: Dosimetry in mammography

C. Cappellini et al., 2008 IEEE Nuclear Science Symposium Conference Record & NIM 607 (2009), 75–77

Dosimetry in mammography is utmost important and this is somehow proven by the ongoing debate on the relevance of mammography screening

...but currently existing instruments are limited:

- Standard **Thermo-Luminescent Detectors** require to be analyzed after examination, degrade with time
- MOSFET detectors** suffer from low stability and degrade with each irradiation
- Ionization chamber devices** need relatively high voltage (cannot be used in contact with the patient), not tissue equivalent

precise measurements of the actual dose being received by a patient without distorting the X-ray beam and introducing any artefacts in the image

Some functional requirements:

- dose rate range ($2 \div 150$ mGy/s)
- dose range (0.5 mGy - 180 mGy)
- sensitivity (5%)
- overall accuracy ($\pm 10\%$)
- tolerance to environmental variation & stability



Prototype qualification

Conceptual design of the prototype tested @ PTW – secondary standard lab for dosimetry:

Scintillator
(tile or fiber)

Ligh guide
Ø 1 mm
clear fiber



FC connector &
SiPM



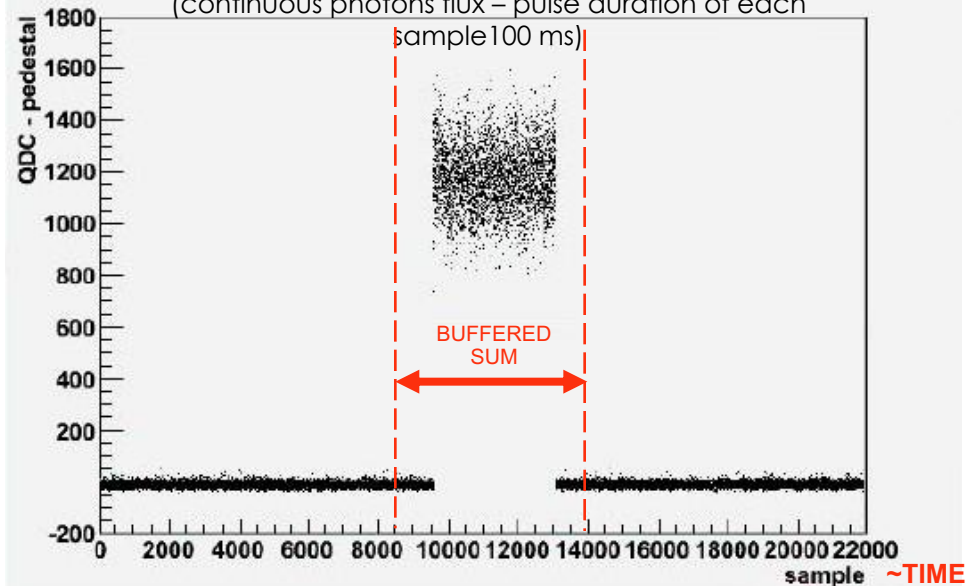
Electronics

PHISYCAL OBSERVABLE:
“buffered” signal sum

Sum of samples signals selected
by an edge detector algorithm
+ left & right buffer

⇒ proportional to the DOSE

Trace plot: typical mammo SiPM output
(continuous photons flux – pulse duration of each

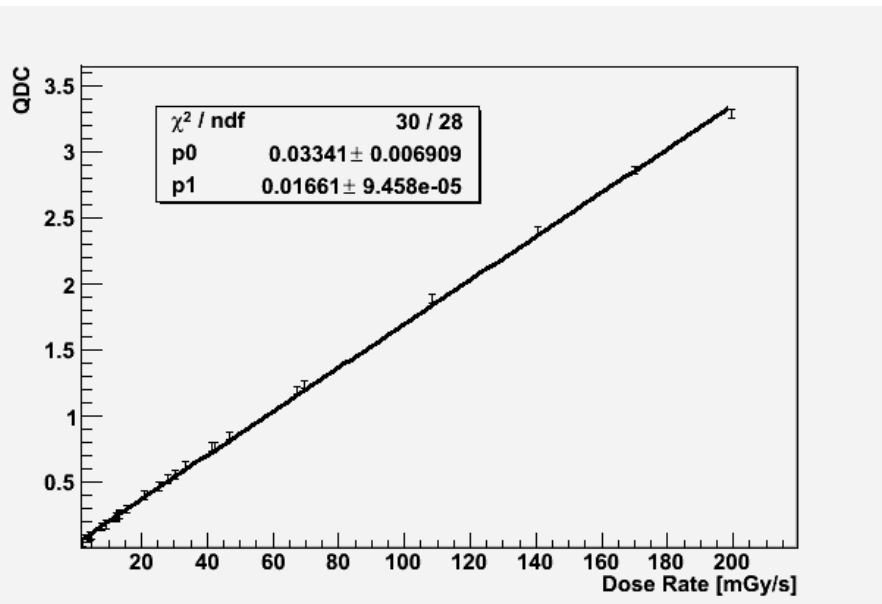


summary of the results

Two different **set-up** (optimized for dynamic range & λ):

- 1mm scintillator tile
 - Blue scintillator fiber
- coupled with MPPC (400 cells, 1x1 mm²)

Irradiation: $0,22 \div 217$ mGy/s



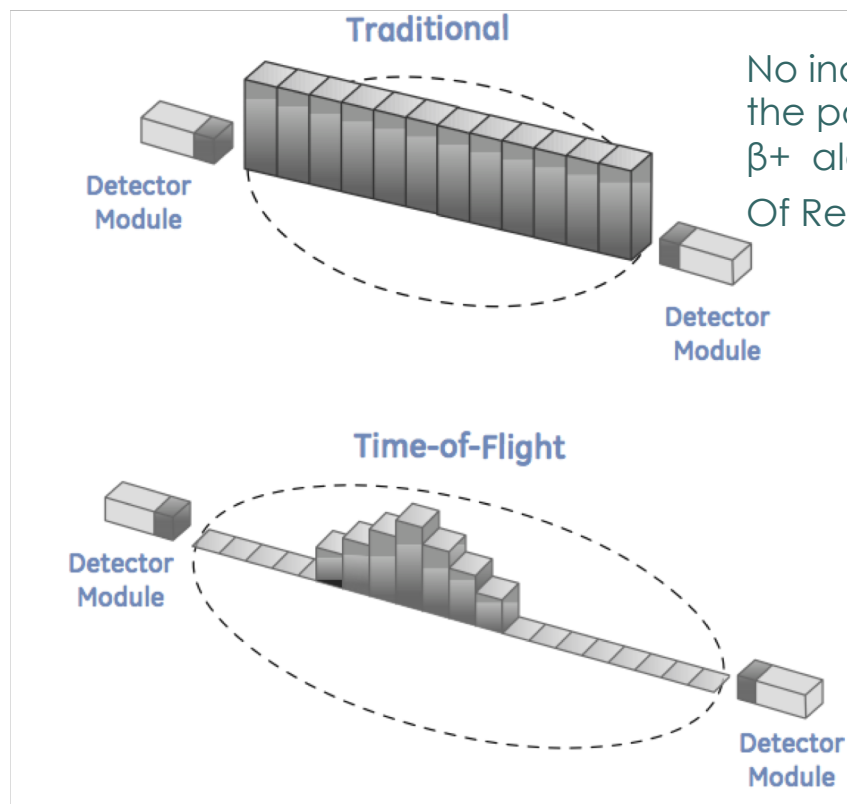
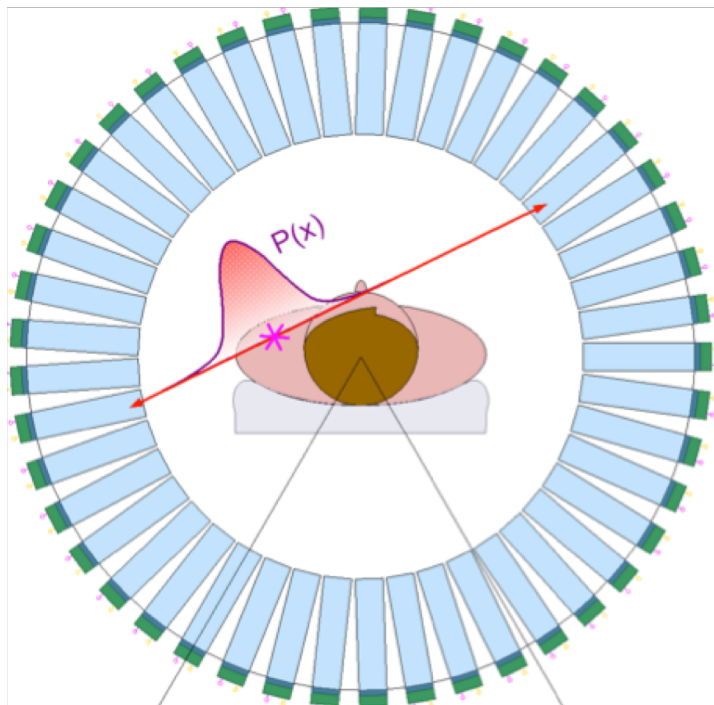
	Fiber + Hamamatsu MPPC
Precision(%)	2.31 ± 0.03
Sensitivity ^A (mGy/s)	2.05 ± 0.03
MDS ^B (mGy/s)	0.458 ± 0.007
Linear Dinamic range (mGy/s)	> 200

^ASensitivity: Precision / system gain

^BMDS: minimum signal distinguishable from the noise

Time-of-flight Positron Emission Tomography (TOF-PET) & LIDAR

M. Conti, Physica Medica (2009) 25, 1-11



The functional imaging tool, based on the detection of pair of γ rays emitted back-to-back by the annihilation of the β^+ emitted by the ^{18}F , chemically bound to FDG

Identify the position of the β^+ along LOR by the difference in the time of arrival of the photons

TOF-PET is a **HOT** topic: 1510 papers in 2008-2013 (Google Scholar) + significant investments by funding agencies & companies

The gain in the image quality between a conventional and a TOF-PET system may be quantified as [Conti]:

$$G = \frac{SNR_{TOF}}{SNR_{non-TOF}} = \sqrt{\frac{D}{c * CTR}}$$

- D = volume being inspected
- c = speed of light
- CTR – Coincidence Time resolution

CTR	G
1 ns	1.6
500 ps	2.3
100 ps	5.2

← Current machines
← **TARGET**

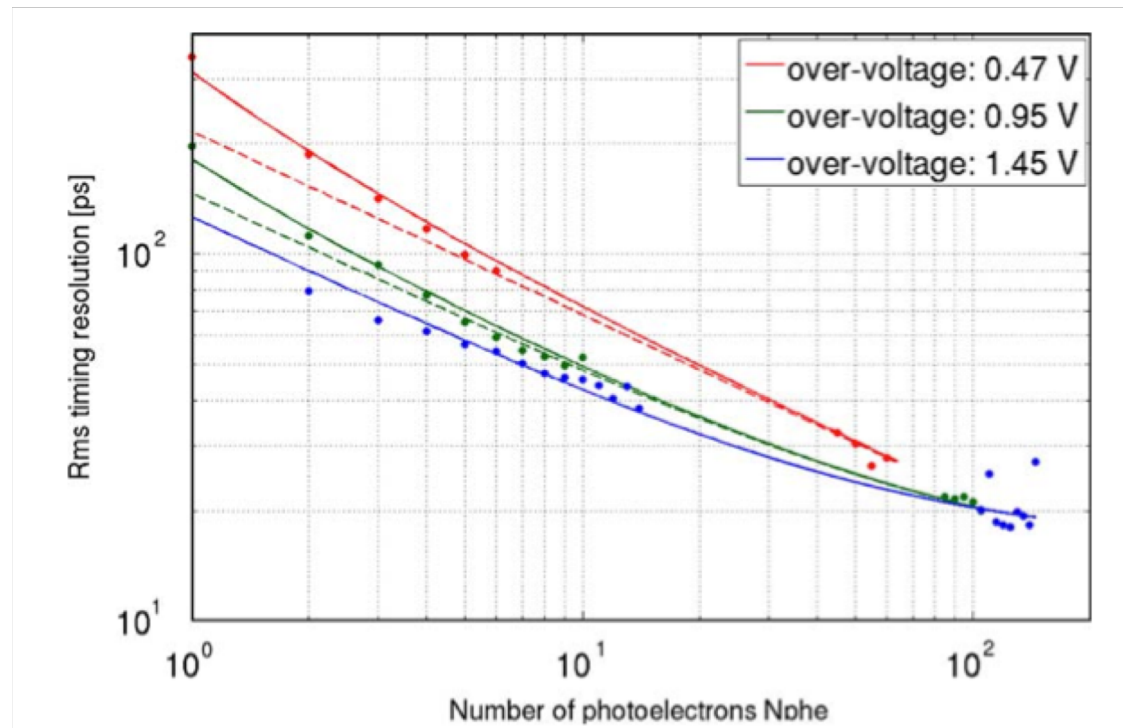
SiPM do play a role, since the timing resolution of a sensor may roughly be written as:

$$\sigma_t = (\text{output signal fluctuations}) / (\text{signal slope})_{\text{trigger}}$$

Exemplary illustration of results obtained with the HAMAMATSU SiPM [R. Vinke et al. NIM A 610 (2009) 188–191]:

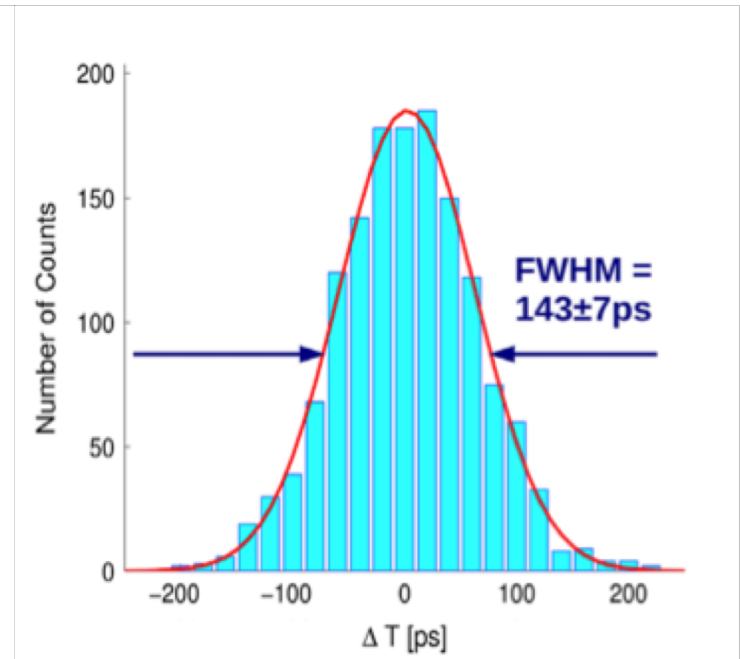
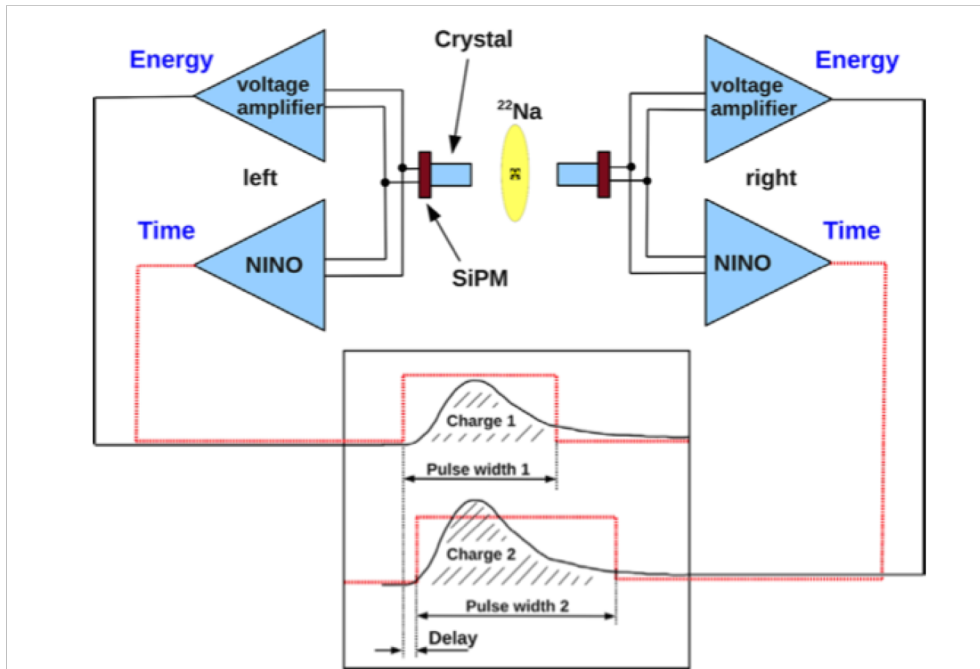
Time resolution
wrt a laser shot
(worth thinking
of it for ranging
& LIDAR)

[1x1 mm², 50 micron cell pitch]



Currently, a SinglePhotonTimingResolution ≈ 35 ps has been reported (Acerbi et al., IEEE Transaction in Nuclear Science, 10.1109/TNS.2014.2347131)

Timing properties of the sensor are not the full story and the scintillator does play a role [S. Gundacker et al., NIM A 737 (2014) 92–100]:



- [3x3 mm², 50 micron cell pitch]
- 2x2x10 mm³ LSO crystal

Actual resolution, accounting as well for the Photon Travel Spread (PTS) resulting by the point-of-interaction and scintillation light time spread

Small animal PET/CT scanning is also a significant market (valued \$790 million in 2012, and estimated to grow at an annual growth rate of 14.5% over the next five years)

❖ The price for different small-animal PET systems ranges between \$400,000 and \$1,200,000, depending on the PET system configuration

❖ No. of crystals/scanner: ~ 30000

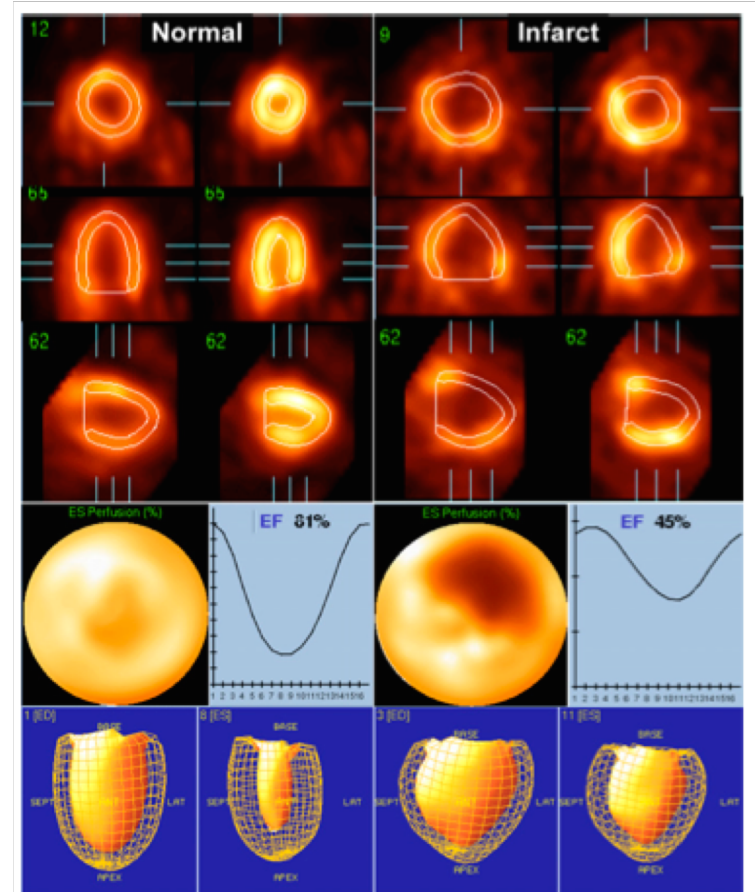


FIGURE 5. Electrocardiogram-gated ^{18}F -FDG studies in normal and infarcted rats obtained using clinical cardiac analysis software QGS (56). Polar maps display end-systolic ^{18}F -FDG uptake. Ejection fractions for normal and infarcted rats are 81% and 45%, respectively. ED = end-diastolic; EF = ejection fraction; ES = end-systolic. (Adapted with permission of (55).)

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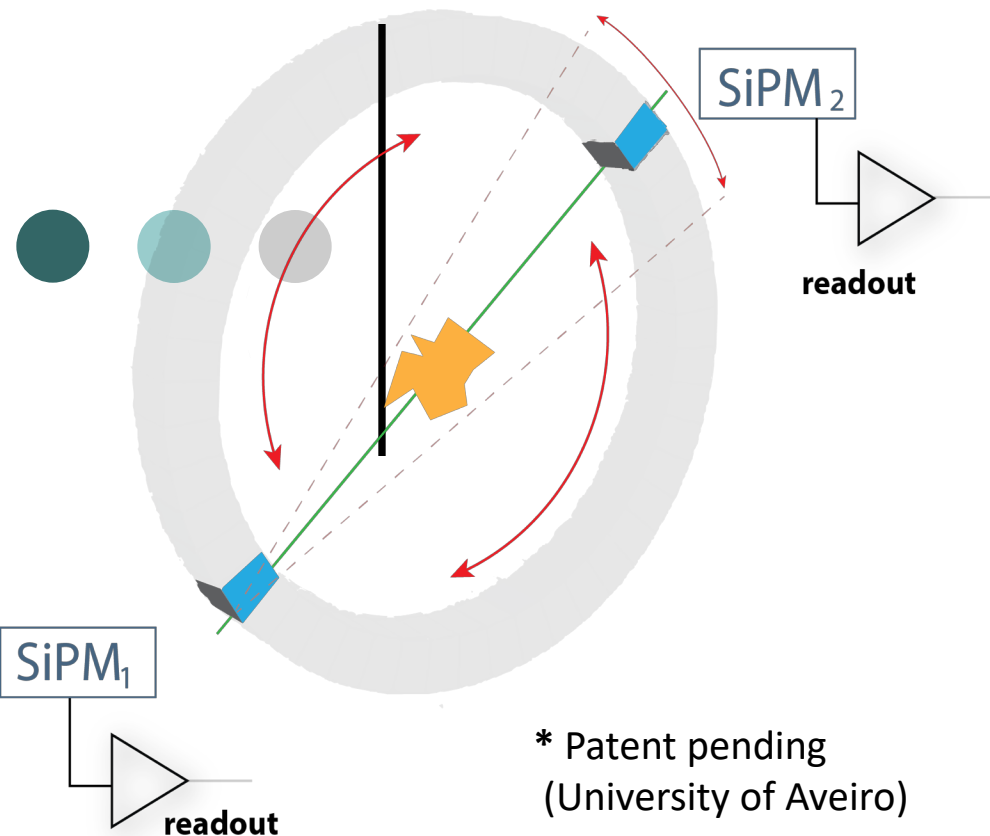
LATEST NEWSFEED ARTICLES

- ▶ Elekta CE Marks Leksell Gamma Knife Icon
- ▶ Oncology professionals discuss new approaches to image-guided

NEWSFEED

Mar 3, 2015
University of Tübingen, Mediso to develop preclinical PET insert for simultaneous PET/MRI

the easyPET concept *



* Patent pending
(University of Aveiro)

- based on a single pair of detectors (LYSO + SiPM)
- detectors mounted on rotating structure with 2 degrees of freedom, allowing reconstruction of source position
- axial FOV: small animals (mice/rats)
- system geometry removes parallax errors, eliminating the need of DOI measurement
- allows highly granular detector assemblies for enhanced performance

easyPET provides a very cost-effective solution for entry level systems, due to the extreme reduction in the nr. of detectors and complexity of the overall apparatus



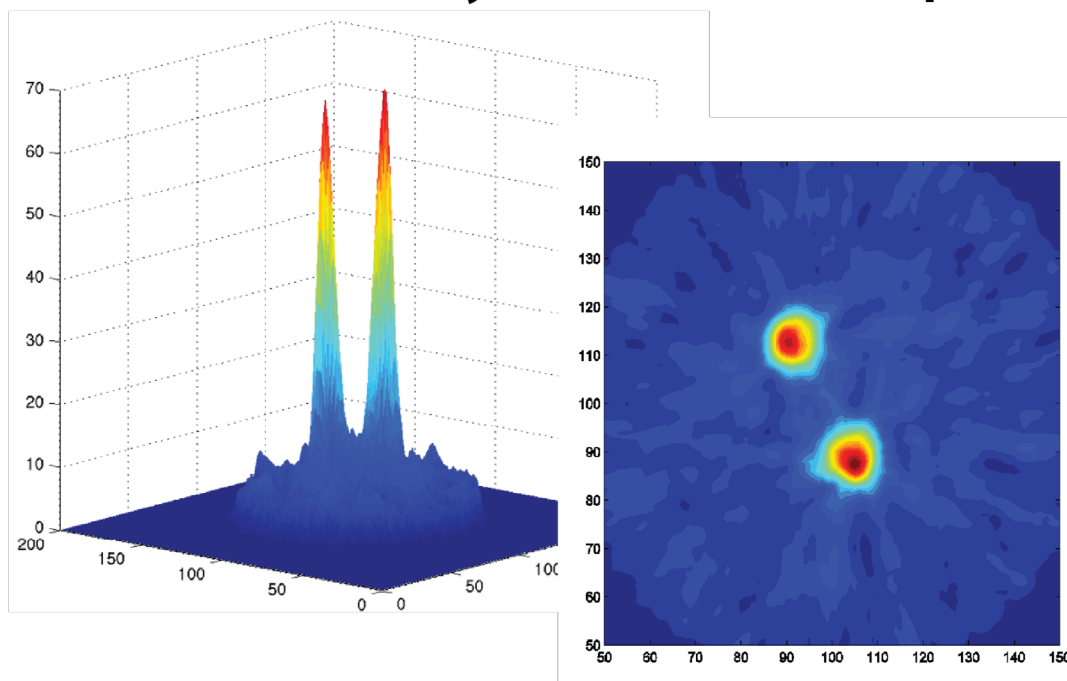
universidade de aveiro

partners:



current status:

{ fully functional
educational system developed *



- Arduino UNO microcontroller
- MATLAB interface: control and online imaging
- Two ^{22}Na sources, 5 μCi
- 2.7 mm \varnothing , 9 mm apart
- forward projection (no filtered reconstruction)
- position resolution < 1.5 mm FWHM, uniform over the whole FOV

* Licensing under way for didactic/educational purposes



universidade de aveiro

partners:



SiPM for Time of Flight LIDAR

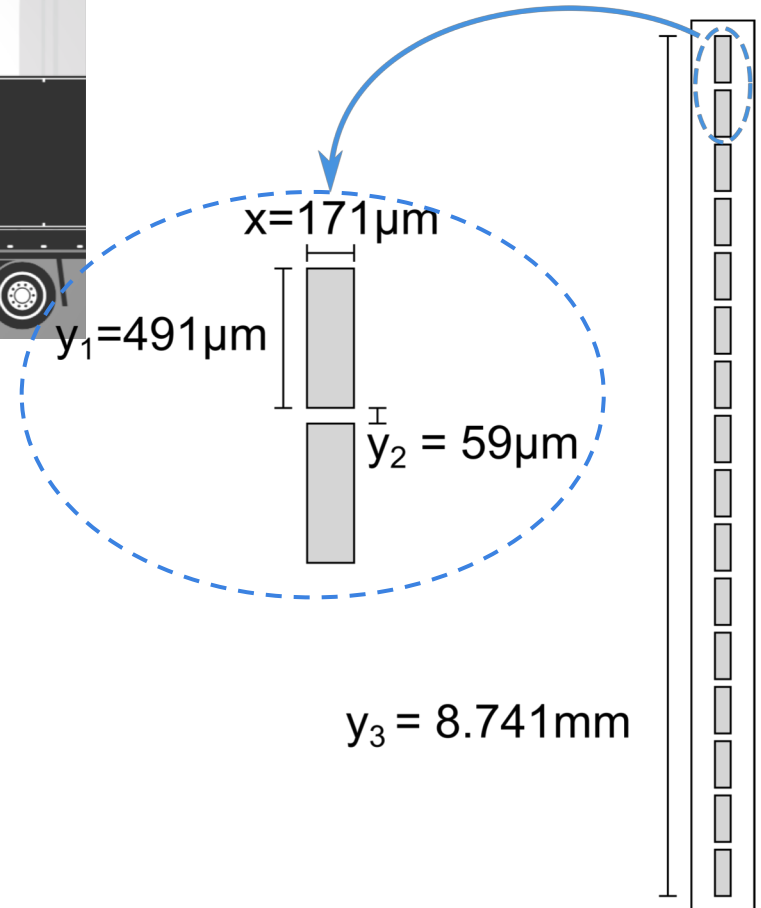
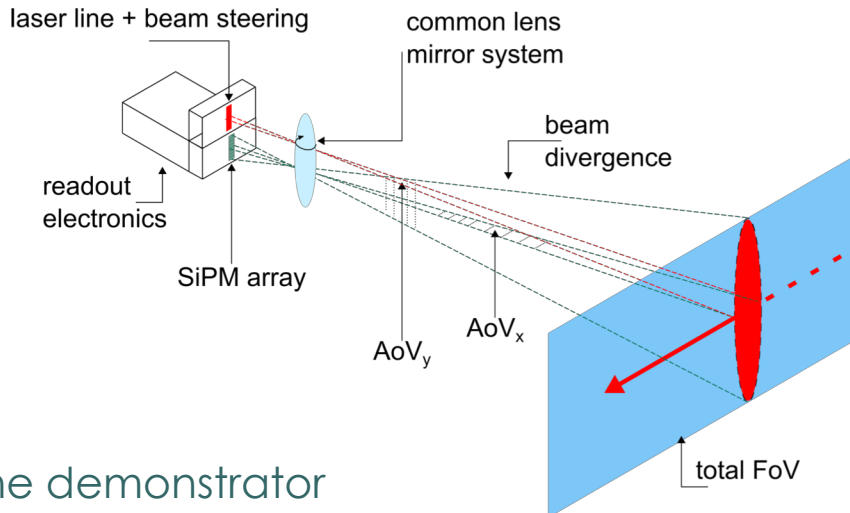
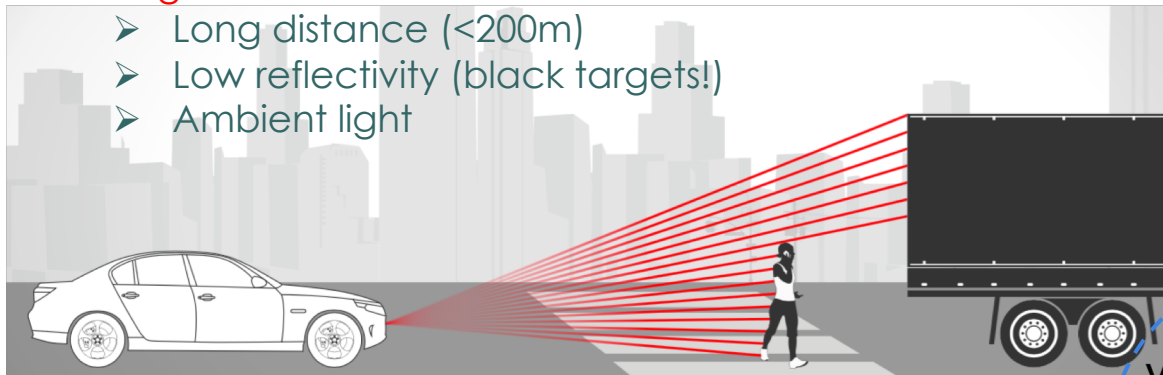


For an excellent paper showing the advantages of SiPM, see
S. Vinogradov, Evaluation of performance of silicon photomultipliers in LIDAR applications, doi:
10.1117/12.2264935

The basic principle

Challenges:

- Long distance (<200m)
- Low reflectivity (black targets!)
- Ambient light

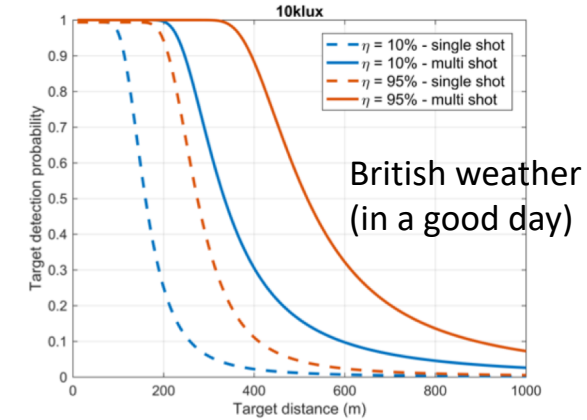
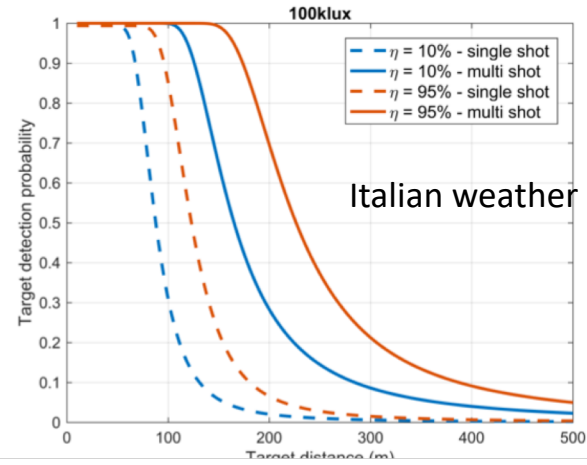


The demonstrator

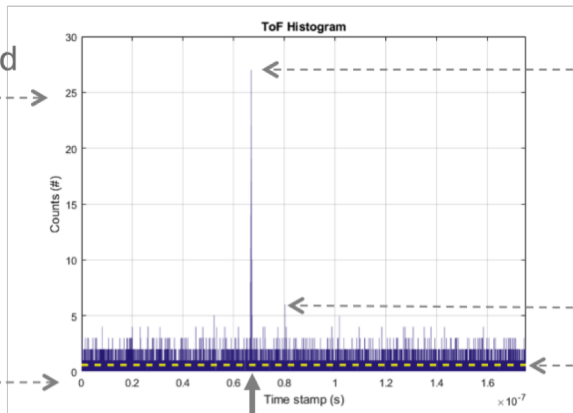
SENSL LIDAR SYSTEM PARAMETERS

Parameter	Value
Array size	1×16
SiPM pixel length x	171 μm
SiPM pixel height y_1	491 μm
Pixel spacing y_2	59 μm
Total array length y_3	8.741 mm
SPAD cells per pixel N_{cells}	133
PDE @ 905 nm	8.4 %
SPAD cell dead time τ_{dead}	23ns
SiPM pixel gain G	10^6
SiPM rise time τ_{rise}	100 ps
Laser divergence	$0.1^\circ \times 5^\circ$
Laser peak power P_{laser}	400 W
Laser pulse width τ_{pulse}	1 ns
Laser pulse repetition rate PRR	500 kHz
Frames per second	30 fps
Optical aperture D_{lens}	22 mm
Scanning angle of view	$80^\circ \times 5^\circ$
Static angle of view $AoV_x \times AoV_y$	$< 0.1^\circ \times 5^\circ$
Angular resolution	$0.1^\circ \times 0.312^\circ$
Optical bandpass $\lambda \pm \Delta\lambda$	$(905 \pm 25) \text{ nm}$

Target Detection Probability



1 Lux = 1 lumen/m²; A 25 W compact fluorescent light bulb puts out around 1700 lumen



Signal peak

Noise peak

Noise average

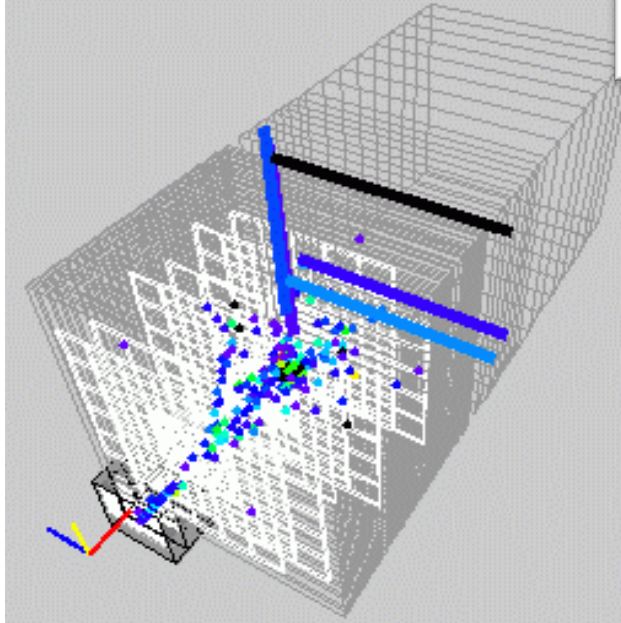
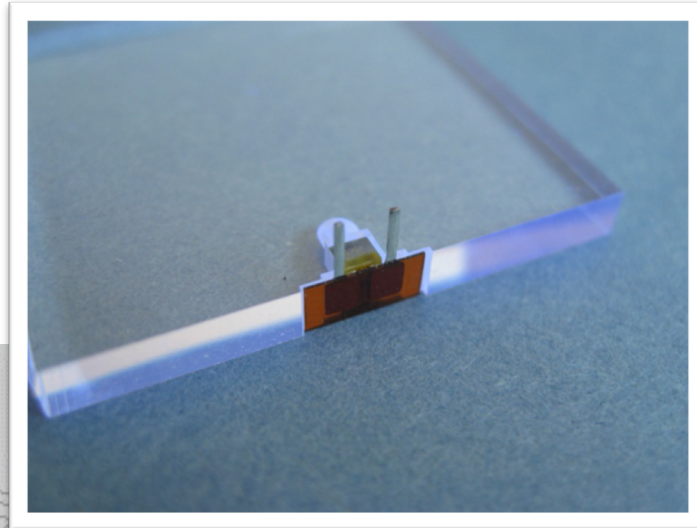
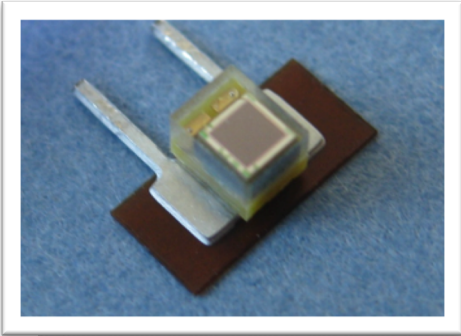
ToF

The returned signal reaches the level of the background noise, and so a multi-shot technique can be used to improve the performance and increase the probability of detection. **Currently, the TOF distribution is built over 20 shots.**

Y-axis: Detected pulse count

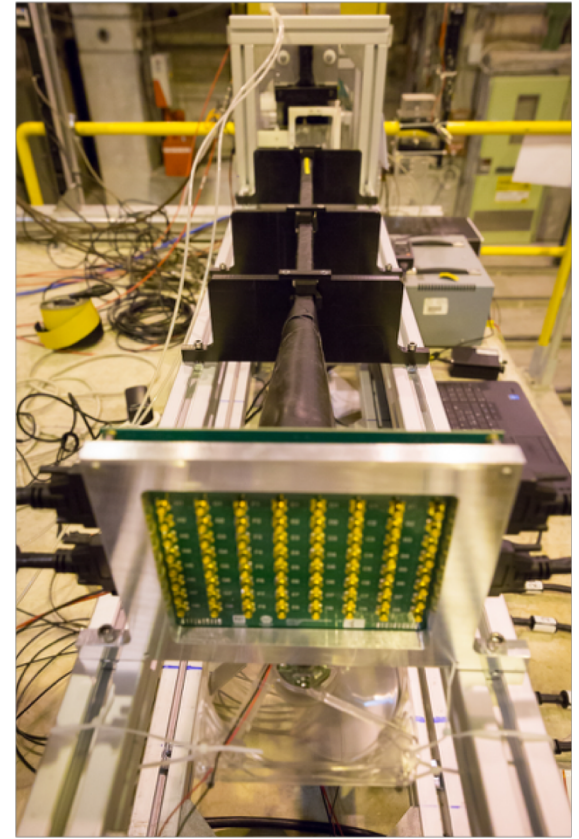
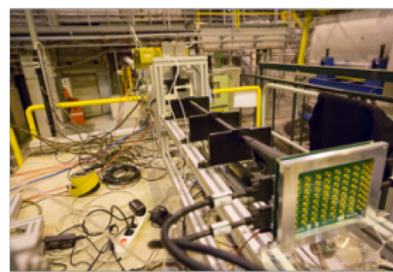
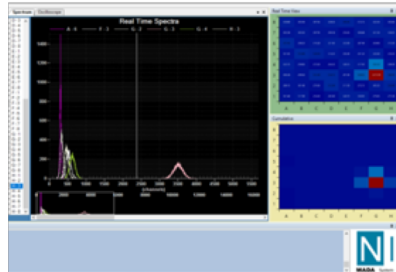
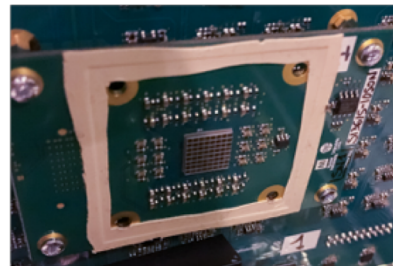
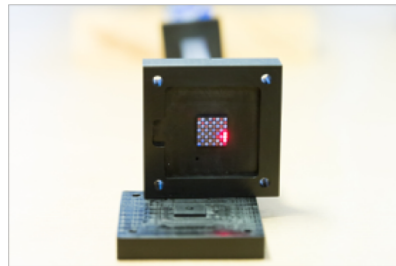
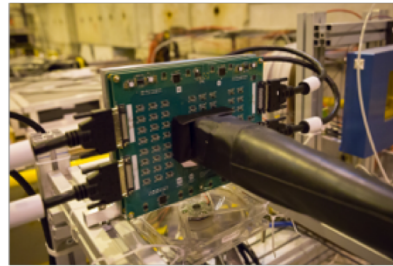
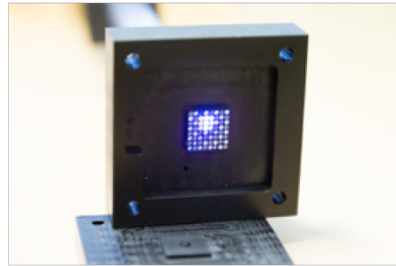
X-axis: TDC timestamp

Last but not least: High Granularity Calorimetry for High Energy Physics [the domain of CALICE, even if we also entered the game]



A SiPM based Dual Readout Calorimeter module (DREAM)
(<http://highenergy.phys.ttu.edu/dream/>)

A small DREAM
by now...

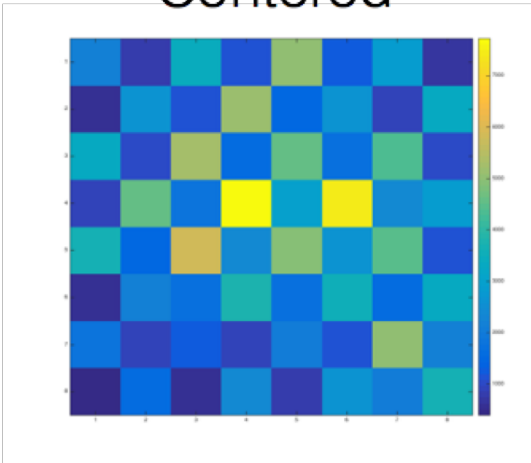


on beam at CERN in October 2016 & July 2017



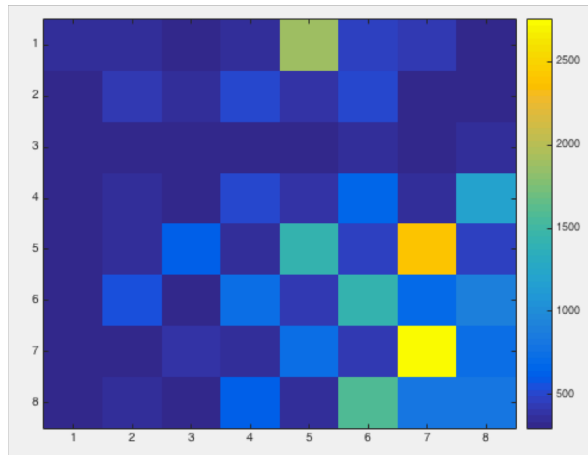
And we made it (and the best is yet to come)!

Centered

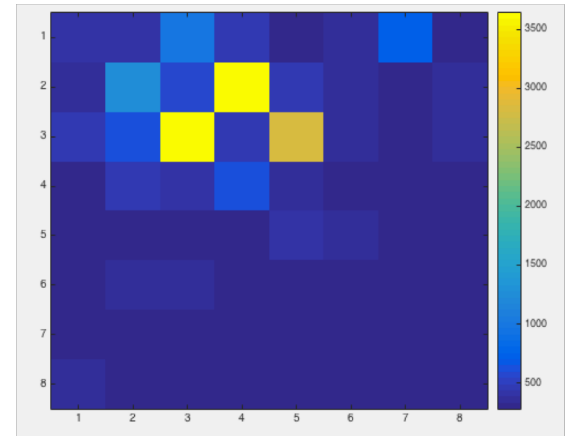


40 GeV electrons

Off-centered



A muon





What did we do since we got started with SiPM, in 2006?

- ❖ RAPSODI, a Framework Program 6 EC project:
 - Real-time dosimetry in mammography (with PTW-Freiburg)
 - Indoor radon concentration (with JP-SMM, Cz)
 - Gamma detection for security (with FORIMTECH-CH)
- ❖ Partnership with CAEN.s.p.a. for the development of a SiPM kit for Science & Education (<http://www.caentechnologies.com/jsp/Template2/CaenProd.jsp?parent=61&idmod=1023>)
- ❖ MODES-SNM, a Framework program 7 EC project on Homeland Security (ARKTIS detectors & CAEN)
- ❖ Two Homeland security projects [KROMEK, AWE (UK Atomic Weapons establishment)]
- ❖ Dual Readout Calorimetry (Texas Tech, Iowa State Uni., INFN, Nuclear Instruments)
- ❖ Radio-guided surgery (Light Point Medical, UK, completed)
- ❖ EasyPET 2D with CAEN and University of Aveiro (3D on the way)
- ❖ Dual Energy Bone densitometry (partnership with an Italian Company)
- ❖ Industrial Automation (Partnership with a Swiss company)
- ❖ Chemiluminescence (in partnership with 2 research institutions from Italy)
- ❖ Dosimetry and QC of radiotherapy machines with scintillating fibers (Ireland)
- ❖ “friendly” relationship with HAMAMATSU Europe & the other producers

Take Home Message: when you see a wave...





Never forget it is made out of drops!

Once more, thank you for listening!

● ● ● | Never forget it is made out of drops!

The banner features a background of green foliage. A dark red horizontal bar is overlaid on the image, containing the conference title in white text. Below the bar, the dates and location are written in white text on a dark background.

International Conference on the Advancement of Silicon Photomultipliers

11.6.2018 - 15.6.2018 Schwetzingen, Germany

<http://icasipm.org>

Once more, thank you for listening!